

1 **Antioxidative and Anti-UV Lignin Carrier for Peptide Delivery**

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16

1 **Abstract**

2 Here, a sustainable antioxidant carrier based on lignin was developed to deliver palmitoyl
3 tripeptide-38. The poly(lignin/PEG/PPG urethane) was polymerized by randomly coupling
4 lignin, PEG and PPG segment blocks using hexamethylene diisocyanate as a crosslinker. The
5 derived poly(lignin/PEG/PPG urethane) loaded with palmitoyl tripeptide-38, referred to as LM,
6 was designed with careful considerations of both intrinsic and extrinsic causes of skin aging
7 and a two-way approach was taken on to effectively target the problem of skin aging. Upon
8 exposure to the ultraviolet irradiation, LM successfully protected the cells by reducing the
9 presence of reactive oxygen species, the damage to the antioxidant enzymes and the expression
10 of MMP-1. Concurrently, LM also promoted the collagen production for skin repair. It was
11 noteworthy that the collagen I content, in cells exposed to ultraviolet irradiation with LM-4 and
12 LM-8 treatment (LM with 4 and 8 $\mu\text{g}/\text{mL}$ palmitoyl tripeptide-38 respectively), exceeded that
13 of the control. Overall, this work successfully demonstrated a sustainable carrier with good
14 antioxidant properties that effectively assisted the uptake of palmitoyl tripeptide-38 by the cells.

15

16 **Keywords:** lignocellulosic biomass, encapsulation, radical oxygen species, ultraviolet
17 irradiation, collagen

18

1 **1 Introduction**

2 Skin aging degenerates the biological functions of skins (such as loss or disorder of collagen
3 and glycosaminoglycans) which results in wrinkles, dyspigmentation, sallow color, dry texture
4 and loss-of-tone. The aging of skin is a complex biological process involving both intrinsic and
5 extrinsic factors.^[1] Genetically programmed intrinsic aging is influenced by proliferation,
6 differentiation and functional activity of skin cells together with the dermal collagen level
7 secreted by dermal fibroblasts. Extrinsic aging is mainly caused by environmental or
8 exogenous factors, including UV radiation, smoking, alcohol consumption and air pollution,
9 etc. Chronic sun (UV) or chemical exposure leads to the formation of various free radical
10 compounds, such as reactive oxygen species (ROS). These free radicals are highly reactive
11 molecules, which tend to damage cellular structures, such as DNA, proteins, and cellular
12 membranes, in our skin. Moreover, such free radicals may also cause locally oxidative stress-
13 related inflammation, tissue damages or even functional disorders.

14

15 Although the necessity of cosmeceutical anti-aging intervention is debatable, the anti-
16 oxidative theory and its approach have been widely accepted by both scientific society and the
17 public. Various antioxidants (e.g. vitamins, lipoic acid, selenium, polyphenols, idebenone) are
18 extensively used as ingredients in dietary and skin care products. There are several types of
19 antioxidants that have different modes of action. One type primarily acts as free radical
20 scavengers that are able to neutralize free radicals directly. Others target the reduction of
21 peroxide content or quench iron to decrease ROS generation and repair oxidized membranes.

22

23 Bioactive peptides have also been used as anti-aging ingredients for skin care applications.
24 Peptides are essential in metabolism processes including regulation of cell functionalization,
25 melanogenesis as well as antioxidative protection of collagen degradation ^[2]. Palmitoyl
26 tripeptide-38 is one of the most well-known peptides being used to reduce skin aging. It can
27 stimulate the synthesis of collagens in skin. Experiments had demonstrated that the peptide was
28 able to decrease skin roughness, wrinkle volume and depth, and increase density and thickness
29 of collagen and elastin fibers in dermis ^[3]. However, a common issue in the topical application
30 of peptides lies in the delivery of such molecules across the stratum corneum. These peptides
31 are still relatively poor in terms of penetration into the skin and uptake by the skin cells.

1 Up to present, many studies have looked into improving the uptake of the peptides by cells.
2 For example, there are the exploration on using chemical, physical and carrier methods.
3 However, chemical and physical approaches are generally not preferred as the usage of
4 chemical enhancers are prone to skin damage and irritation ^[4]. Physical approach can be
5 complicated to perform, the application can be limited to charged molecules and skin damage
6 can occur as well ^[4]. Microneedles has received much attention as a potential technique to
7 overcome the barrier and being minimally invasive ^[5] ^[6]. Another method is to utilize the
8 transdermal enhanced peptide in which the selected peptides have the ability to overcome the
9 cell membrane impermeability ^[4, 7].

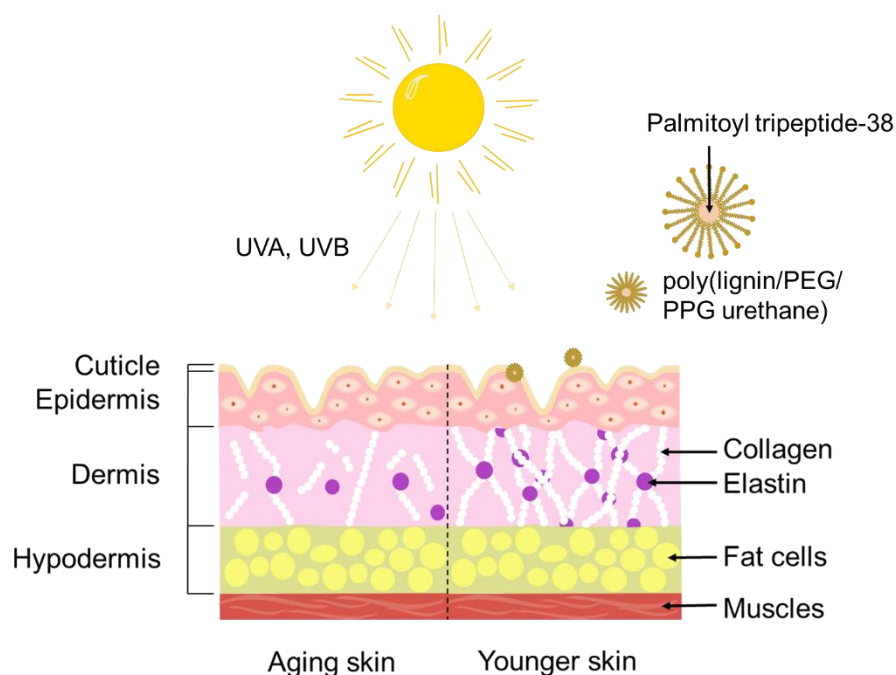
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11 With the increasing demand for conventional petroleum-based materials over the past several
12 decades, rising environmental pollution and future depletion of fossil fuels have motivated
13 researchers to look into sustainable bio-renewable polymers. Lignocellulosic biomass is
14 regarded as the most promising alternative in light of natural abundance and renewability.
15 Being the second most abundant natural polymer, lignin is readily available on a large scale as
16 the byproduct of pulp and paper industry. The recent advancement in the field of lignin-based
17 processing coupled with lignin inherent physiochemical characteristics make it to be a potential
18 well-deserved contender for high value biopolymers. The unique properties of lignin, such as
19 their high activity in binding sodium salts of cholic acid, antiviral and antibacterial activities,
20 have gained great attention for biomedical applications ^[8]. Additionally, lignin is an effective
21 free radical scavenger. It consists of aromatic monomers, and it can be rationalized as the
22 polymerization of three phenylpropanoid monomers: para-coumaryl alcohol, coniferyl alcohol,
23 and sinapyl alcohol. These functional groups on lignin could assist to terminate the oxidation
24 propagation reaction via hydrogen donation. As such, lignin is able to stabilize the reactions
25 induced by oxygen and its radical species, and also inhibit enzyme activities associated with
26 the generation of superoxide anion radicals in cancer cells to obstruct their proliferation ^[9]. In
27 our previous studies, we have demonstrated that lignin-based nanofibers showed good
28 antioxidant activities and promoted the growth of different cell types ^[10]. Due to its antioxidant
29 activity, lignin has become a promising sustainable material for applications in cosmetic,
30 pharmaceutical and food processing industries.

31

32

1 In this study, we developed lignin-based copolymers for the delivery of palmitoyl tripeptide-
2 38 (Figure 1). Poly(lignin/polyethylene glycol (PEG)/polypropylene glycol (PPG) urethane)
3 was synthesized from lignin, PEG and PPG. The chemical and thermal properties of the lignin
4 based copolymers were characterized by NMR, GPC and DSC. Poly(lignin/PEG/PPG urethane)
5 is capable of forming micelle in aqueous solutions, and particle size and critical micelle
6 concentration (CMC) of the solution were studied. Performance evaluation of the
7 poly(lignin/PEG/PPG urethane) as a carrier was conducted by encapsulating palmitoyl
8 tripeptide-38 in the micelles. Human skin fibroblasts (HSF) treated with UVA irradiation were
9 used as the cell aging model. Cell proliferation, collagen production, reactive oxygen species
10 (ROS) content, the activity of diminished superoxide dismutase (SOD), catalase (CAT),
11 glutathione peroxidase (GSH-px) and lactate dehydrogenase (LDH), malondialdehyde (MDA)
12 production, and matrix metalloproteinases 1 (MMP-1) expression were measured to assess the
13 efficacy of delivering the anti-aging peptides.



14

15 Figure 1: Illustration of poly(lignin/PEG/PPG urethane) assisting the uptake of palmitoyl
16 tripeptide-38 by the cells leading to skin repair despite the ultraviolet radiation

17

18

19 2 Materials and Methods

1 **2.1 Materials**

2 All chemicals were purchased from Sigma-Aldrich Chemicals and used as received except
3 where noted. Kraft lignin (average molecular weight = 5,000 g/mol) was dried at 105 °C in
4 oven for 12 hours before use. The molecular weight of PEG and PPG were 2,000 g/mol, and
5 2,200 g/mol, respectively.

6 Dulbecco's Modified Eagle's Medium (DMEM) High Glucose, fetal bovine serum (FBS), and
7 trypsin were purchased from Gibco Life Technologies (Carlsbad, CA, USA). Dimethyl
8 sulfoxide (DMSO) and CCK8 kit were purchased from AMRESCO LLC (USA); ROS kit,
9 SOD kit, MDA kit, CAT kit, GSH-px kit and LDH kit were purchased from Nanjing Jiancheng
10 Bioengineering Institute (Nanjing, China); Human type I collagen ELISA kit and Human type
11 III collagen ELISA kit were purchased from RD company pack; MMP-1 antibody and β -actin
12 antibody were purchased from abcam (Cambridge, UK). Palmitoyl tripeptide-38 was
13 purchased from Croda.

14

15 **2.2 Synthesis of poly(lignin/PEG/PPG urethane)**

16 Poly(lignin/PEG/PPG urethane) was synthesized from the lignin, PEG and PPG with weight
17 ratios of lignin:PEG:PPG = 5:63:32, using hexamethylene diisocyanate (HMDI) as a coupling
18 reagent (Scheme 1). The amount of HMDI added was equivalent to the reactive hydroxyl
19 groups in the solution. Lignin, PEG, and PPG were vacuum dried at 50 °C overnight, in a 250
20 ml two-neck flask. Then 0.20 g HMDI was added into the mixture and stirred for 1 hour. Next
21 20 ml of chloroform was added into the flask and the reaction mixture continued to stir for 24
22 h at 70 °C, under a nitrogen atmosphere. After reaction, diethyl ether was utilized to precipitate
23 the resultant polymers. The final product was obtained with yield of 70%.

24

25 **2.3 Characterization of poly(lignin/PEG/PPG urethane)**

26 NMR spectrum of poly(lignin/PEG/PPG urethane) was measured at room temperature using
27 Bruker AV-400 NMR spectrometer in CDCl_3 solvent. Molecular weight (M_n and M_w) and
28 polydispersity index of polymer were analyzed by Waters gel permeation chromatography
29 (GPC, a Shimadzu SCL-10A and LC-8A system equipped with two Phenogel 5 mm 50 and
30 1000 Å columns in series and a Shimadzu RID-10A refractive index detector) using HPLC
31 grade tetrahydrofuran as an eluent. The flow rate of tetrahydrofuran eluent was 1.0 ml/min at

1 25 °C. The average molecular weights were determined with a calibration based on linear
2 poly(methyl methacrylate) standards.

3 Thermal behavior of the polymer was also investigated and performed on Thermogravimetric
4 analysis (TGA, Q500, TA Instruments, USA) and differential scanning calorimeter (DSC,
5 Q100, TA Instruments, USA). For TGA, the sample was heated at 20 °C/min from room
6 temperature to 600 °C in a dynamic nitrogen atmosphere (flow rate = 60 ml/min). DSC is
7 equipped with an auto cool accessory and calibrated using indium. The following protocol was
8 used for test: heating from -50 °C to +100 °C at 20 °C/min, holding at +100 °C for 5 min,
9 cooling from +100 °C to -50 °C at 20 °C/min, and finally reheating from -50 °C to +100 °C at
10 20 °C/min. Melting temperature (T_m) and melting enthalpy change (ΔH_m) was determined from
11 the endothermic melting peak from the second heating run.

12 Particle size of poly(lignin/PEG/PPG urethane) in water and its critical micelle concentration
13 (CMC) were determined using a Malvern Zetasizer, NANO ZS (Malvern Instruments Limited,
14 U.K.) equipped with a 4 mW He–Ne laser operating at a wavelength of 633 nm. Measurements
15 were carried out in a polystyrene cell at 25 °C. A series of poly(lignin/PEG/PPG urethane)
16 solutions ranging from 0.5 wt% to 0.0001 wt% were prepared from an aqueous stock solution
17 of 1 wt%. Data processing was carried out with a computer attached to the instrument. The
18 CMC value was determined by plotting a graph of the count rate versus the logarithmic
19 copolymer concentration. The stability of 0.5 wt% poly(lignin/PEG/PPG urethane) in
20 phosphate-buffered saline (PBS) and medium was measured on day 0, 1, 3, 5, 7, 10 and 14.
21 The morphology of poly(lignin/PEG/PPG urethane) micelle was characterized by transmission
22 electron microscopy (TEM).

23 The antioxidant activity of the poly(lignin/PEG/PPG urethane) was evaluated by 1,1-diphenyl-
24 2-picrylhydrazyl (DPPH) assay ^[11]. 10 mg of the copolymer were placed in 15 ml glass vials.
25 A 60 μ M DPPH solution was prepared in methanol, and 10 ml of such solution was added into
26 each vial. DPPH free radical content was measured by monitoring the absorbance changes at
27 517 nm at each time point. All samples were prepared in triplicate. The antiradical activity was
28 measured as % inhibition of free radicals by measuring the decrease in absorbance compared
29 to control solutions. Pluronic F127 was used as control.

30

31 **2.4 Cell culture**

1 Human skin fibroblasts cell line (HSF) was purchased from the Chinese Academy of Sciences
2 Shanghai cell bank (Shanghai,China). Cells were maintained in DMEM supplemented with 10%
3 FBS, 1% penicillin and 1% streptomycin in a cell incubator with 5% CO₂ at 37 °C.

4 **2.5 Cytotoxicity evaluation**

5 Cytotoxicity of the poly(lignin/PEG/PPG urethane) was evaluated with cell titer blue assay on
6 NIH/3T3 cells. 5000 cells were seeded and incubated at 37°C under 5% carbon dioxide and
7 95% relative humidity atmosphere for 24 h. Poly(lignin/PEG/PPG urethane) was introduced to
8 the wells and allowed to incubate for 24h, 48h or 72h. Subsequently, cell titer blue assay was
9 added and incubated for another 3h before measurements were taken at excitation and emission
10 wavelength of 560nm and 590nm respectively.

11

12 **2.6 UVA irradiation**

13 HSF cells were seeded on culture dishes washed with phosphate-buffered saline (PBS) once
14 after incubation and then exposed to UVA (10 J/cm²). UVA irradiated doses were calculated
15 by ultraviolet intensity measurement (UV340B, China Sampo Ltd. Shenzhen, China). After
16 exposure to UVA, cells were incubated in DMEM for 24 h. In parallel, control cells were
17 treated under the same conditions without UVA irradiation.

18

19 **2.7 Intracellular ROS measurement**

20 Intracellular ROS level was evaluated by 2,7-dichlorofluorescein diacetate (DCFH-DA) assay.
21 HSF cells were seeded in 96-well culture plates (80% filled) at a density of 5×10^4 cells/well
22 and incubated at 37 °C. After irradiation with 10 J/cm² UVA, the cells were incubated with
23 different concentrations of palmitoyl tripeptide-38 for 24 h. Subsequently, cells were further
24 incubated with 50 μL 10 μmol L⁻¹ DCFH-DA for 20 min and washed three times with serum-
25 free DMEM. The fluorescence intensity was detected at 488 nm excitation and 525 nm
26 emission and quantified using a fluorescence microplate reader (Synergy HT, BioTek, USA).

27

28 **2.8 Measurement of MDA content**

1 Oxygen radicals elicit membrane peroxidation and MDA formation, which are detrimental to
2 cellular function. MDA production was evaluated in cell lysates using the MDA reagent kit
3 according to the manufacturer's instructions.

4

5 **2.9 Determination of the activities of SOD, CAT and GSH-Px**

6 HSF cells were seeded in 96-well plates at the density of 1×10^5 cells/well with or without
7 treatment with palmitoyl tripeptide-38 for 24 h followed by UVA irradiation. The activities of
8 SOD, CAT and GSH-Px were determined using relevant commercial kits in accordance with
9 the instruction manual.

10

11 **2.10 Cell viability assay**

12 Cellular viability was assessed with cell counting kit-8 and lactate dehydrogenase (LDH)
13 release assays. HSF cells were trypsinized, seeded at 5×10^4 cells/well in 96-well plates,
14 exposed to UVA irradiation and incubated for 72 h. The cells were then treated with different
15 concentrations of palmitoyl tripeptide-38. Subsequently, 20 μ l of CCK-8 solution was added
16 into each well and 100 μ l of serum-free medium was added into the control cells. After
17 incubation for 1 h at 37 °C, absorbance at 450 nm for each well was measured using a
18 microplate reader (Synergy HT, BioTek, Winooski, VT, USA). LDH release was monitored
19 with the Cytotoxicity Detection Kit LDH in cell-free culture supernatants.

20

21 **2.11 Western blotting analysis**

22 Cells were seeded in 96-well plates at the density of 1×10^5 cells/well with or without treatment
23 with palmitoyl tripeptide-38 for 24 h after UVA irradiation. The treated cells were washed
24 twice with cold PBS and homogenized in 1ml RIPA protein lysis buffer at 12 000 rpm for 15 min at
25 4 °C. Protein concentration was measured by a BCA protein assay kit. Aliquot of the
26 supernatant, containing equal amounts of proteins, were electrophoresed on 10% separation gel
27 and 5% concentrated gel and then transferred onto nitrocellulose membranes (Amersham
28 Pharmacia Biotech., England, UK). The membranes were washed twice with Tris/buffered
29 saline (TBS) and blocked in the 5% skimmed milk powder of blocking liquid for 1h at 37°C.

1 Subsequently, they were transferred into TBST and incubated for 2 h at room temperature with
2 appropriate concentrations of primary antibodies (β -actin was 1: 3000 dilution, MMP-1 was 1:
3 1000 dilution). The probed membranes were washed with TBST three times, 10 min for each,
4 and then incubated with secondary antibodies for 2 h in the same way. Western blot was
5 repeated three times under the same conditions independently for the assessment of intra-
6 experimental variability. Immunobands were detected on ECL reagents and quantified using
7 Tanon T600 image analysis system (Shanghai Tanon Technology Ltd. Shanghai, China). β -
8 actin was considered as a loading control.

9

10 **2.12 Collagen content measurement**

11 Cells were seeded in 96-well plates at the density of 1×10^5 cells/well with or without treatment
12 with palmitoyl tripeptide-38 for 24 h after UVA irradiation. The content of human type I
13 collagen and type III collagen were determined using relevant commercial kits in accordance
14 with the instruction manual.

15

16 **2.13 Statistical analysis**

17 Each experiment was repeated at least 3 times. All data were expressed as mean \pm standard
18 deviation ($\bar{x} \pm s$). The significance test was analyzed by SPSS19.0 software. Differences
19 between groups were analyzed by variance analysis, $P < 0.05$ or $P < 0.01$ was considered as a
20 significant.

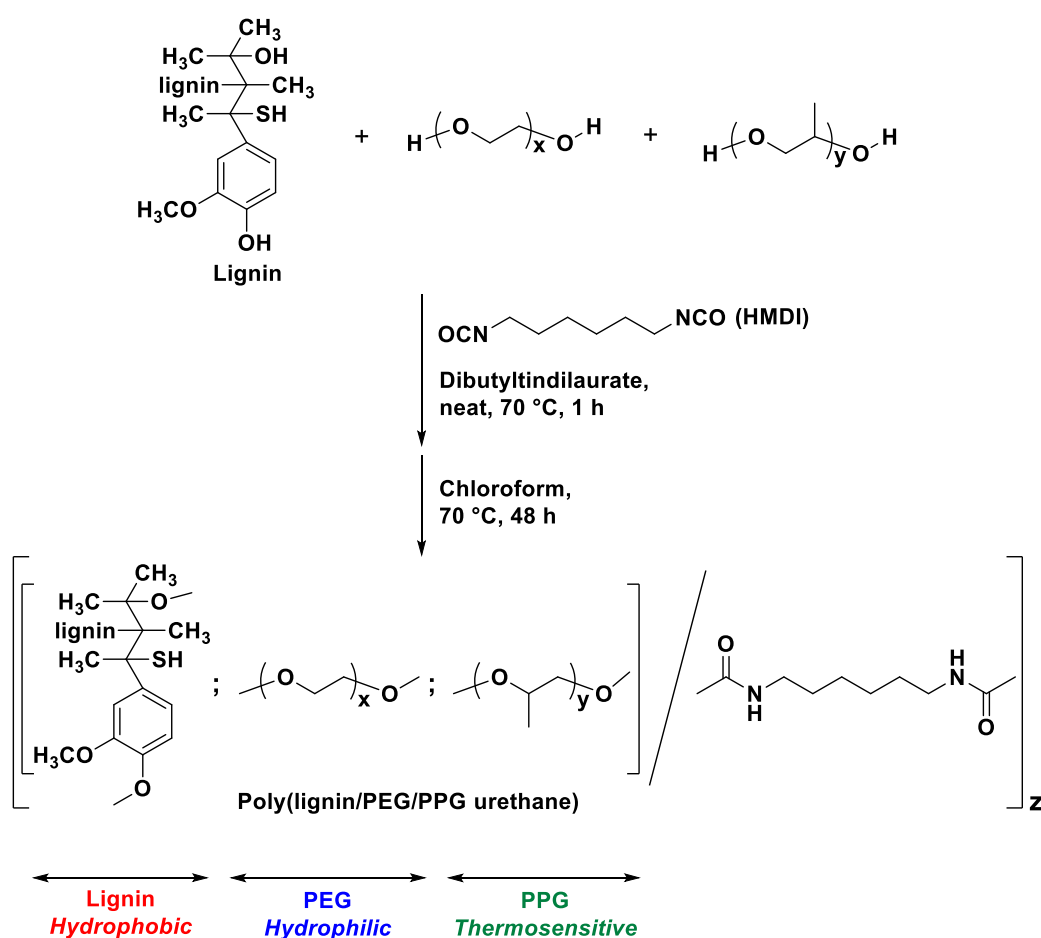
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22 **3 Results and discussion**

23 **3.1 Synthesis and characterization of poly(lignin/PEG/PPG urethane)**

24 Kraft lignin is difficult to dissolve in water (pH 7) and many organic solvents, which limits its
25 surface modification and applications. In this study, we reported a simple method to synthesize
26 water soluble lignin-based polyurethane. Poly(lignin/PEG/PPG urethane) was polymerized by
27 randomly coupling lignin, PEG and PPG segment blocks using HMDI with dibutyltin dilaurate
28 as the catalyst. The synthesis route of the poly(lignin/PEG/PPG urethane) is shown in Scheme
29 1. The chemical structure of poly(lignin/PEG/PPG urethane) prepared in $CDCl_3$ was verified

1 by ^1H NMR (Figure S1). All proton signals belonging to PEG and PPG segments were
 2 observed (δ 4.92-4.87 (m, CH of PPG unit), 4.46-4.44 (m, CH_2 of PPG unit), 4.21-4.19 (t, CH_2
 3 of PEG unit), 3.79-3.76 (t, CH_2 of PPG unit), 3.66-3.64 (m, CH and CH_2 of PPG unit, CH_2 of
 4 PEG unit), 3.58-3.39 (m, CH_2 of PPG unit), 1.14-1.12 (CH_3 of PPG unit)). The signals of
 5 HMDI were identified at 3.16-3.13 ppm (NHCH_2), 1.50-1.47 ppm (NHCH_2CH_2), 1.33-1.30
 6 ppm ($\text{NHCH}_2\text{CH}_2\text{CH}_2$). The signal of lignin methoxyl groups (3.7 ppm) was overlapped with
 7 the peaks of PPG and PEG. The molecular weight of poly(lignin/PEG/PPG urethane) was 9.8
 8 kDa for M_n and 11.7 kDa for M_w , determined by GPC. The obtained poly(lignin/PEG/PPG
 9 urethane) was soluble in water and many commonly used organic solvents (e.g. chloroform,
 10 THF, acetone), forming uniform light yellow solutions (Figure S2).



11
 12 Scheme 1 Illustration of the synthesis reaction

13 The thermal properties of poly(lignin/PEG/PPG urethane) were characterized by TGA and
 14 DSC. Under N_2 atmosphere, kraft lignin thermally decomposed very slowly. Its decomposition
 15 temperature (T_d , @ 5% weight loss) was 260°C and large amount of carbon residual (almost
 16 60%) remained even at 500°C (Figure S3). Unlike raw lignin, poly(lignin/PEG/PPG urethane)
 17 showed similar decomposition profile as PEG-PPG copolymers (Figure S4A). T_d and

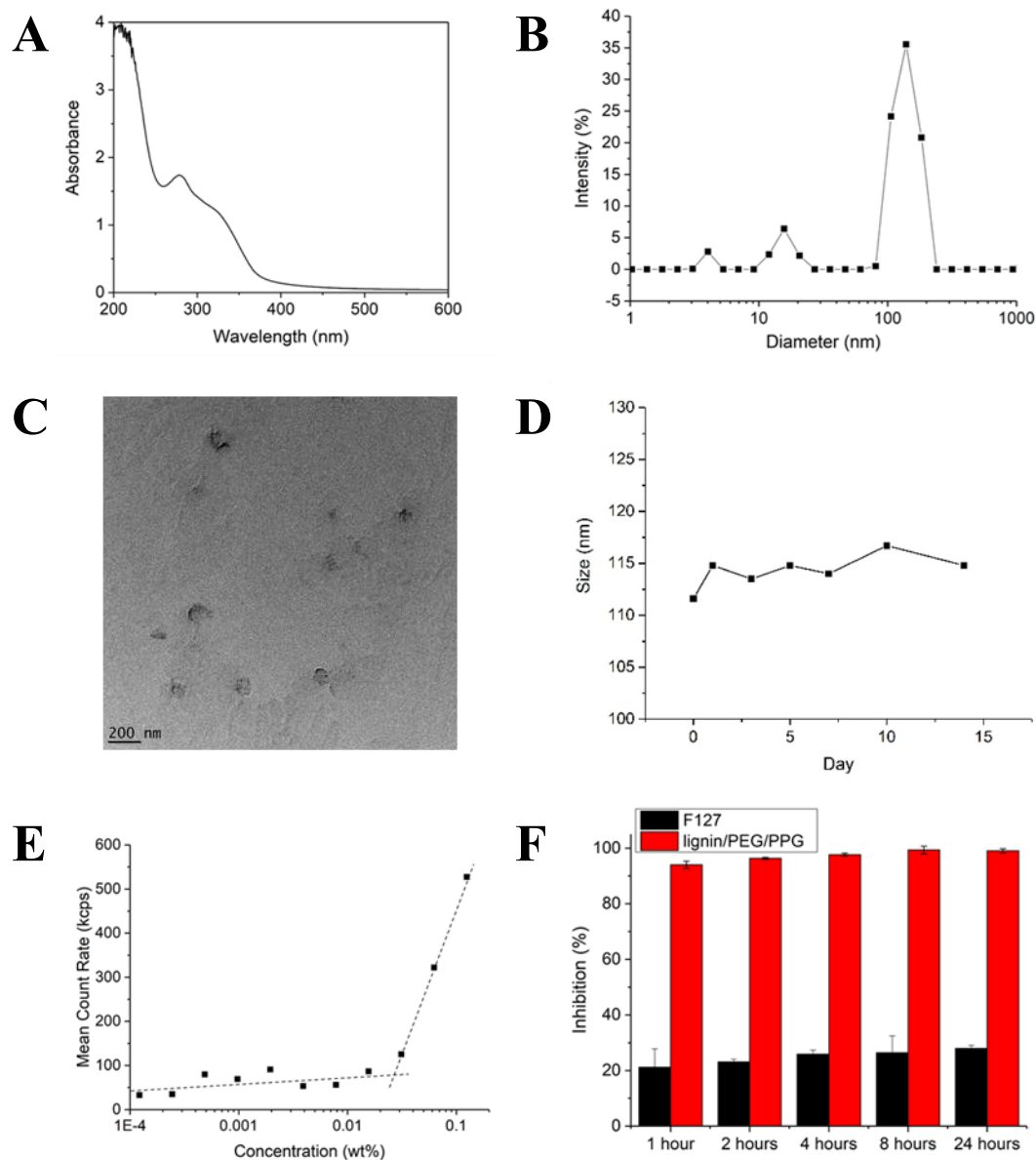
1 derivative peak temperatures of poly(lignin/PEG/PPG urethane) were found at 337 °C and
2 417 °C respectively. The amount of carbon residual at 500 °C was only 3.2%. DSC result shows
3 that the poly(lignin/PEG/PPG urethane) was a semi-crystalline polymer with a melting
4 temperature (T_m) of 44 °C and an enthalpy of 124 J/g (Figure 5B). The thermal behaviour was
5 similar to the commonly used PEG-PPG copolymers, pluronic F127, which has a T_m of 49 °C
6 and an enthalpy of 112 J/g (Figure S5).

7
8

9 **3.2 UV absorption capability of poly(lignin/PEG/PPG urethane)**

10 The results of the UV spectroscopy shows that poly(lignin/PEG/PPG urethane) (Figure 2A)
11 had broad absorbance across UV-A to UV-C ranges. It strongly absorbed within the more
12 harmful UV-C range (200 to 280 nm) and UV-B ranges (280 to 315 nm). It also absorbed in
13 the UV-A (315 to 400 nm). A characteristic absorption maxima was visible at around 280 nm
14 which could be attributed to the abundance of aromatic phenolic groups present in the structure
15 of lignin. This demonstrated good UV performance of the material.

16



1

2 Figure 2 Graph displaying the absorbance of poly(lignin/PEG/PPG urethane) against different

3 wavelengths (A); Size distribution of 0.5 wt% poly(lignin/PEG/PPG urethane) aqueous

4 solution obtained by DLS (B); TEM image of 1 wt% poly(lignin/PEG/PPG urethane) (C);

5 Stability of poly(lignin/PEG/PPG urethane) in PBS measured across 14 days (D); Mean count

6 rates (kcps) as a function of poly(lignin/PEG/PPG urethane) concentration (E); Free radical

7 inhibition (an indication of the antioxidant activity) of poly(lignin/PEG/PPG urethane) and

8 F127 (control) measured by DPPH assay (F)

9

10

11 **3.3 Micelle properties of poly(lignin/PEG/PPG urethane)**

1 The micelle properties of the water-soluble poly(lignin/PEG/PPG urethane) were studied with
2 the use of DLS. DLS is a commonly used technique to detect particle size in colloidal
3 dispersions. Poly(lignin/PEG/PPG urethane) was dissolved in DI water to form 0.5 wt%
4 aqueous solution, and DLS results shows that the average particle size of the copolymer was
5 96.6 nm with a PDI of 0.46 (Figure 2B), indicating that the poly(lignin/PEG/PPG urethane)
6 was able to form micelles in water. The TEM image (Figure 2C) shows that most of the round
7 micelles exhibited uniform size (~100 nm), which is consistent to the DLS result. Additionally,
8 it was found that micelles formed from poly(lignin/PEG/PPG urethane) was relatively stable
9 for the tested period (Figure 2D and S6). The micelles formed in PBS displayed size that ranged
10 between 111nm and 117nm. Hence, the critical micelle concentration (CMC) determination
11 was carried out for the poly(lignin/PEG/PPG urethane) at 25 °C. Besides particle size, DLS is
12 also suitable for studying micellization phenomena and determination of the CMC values. This
13 experiment was conducted by varying the aqueous polymer concentration in the range of
14 0.0001 to 0.5 wt%. The mean count rates (representing the average scattering intensity) as a
15 function of poly(lignin/PEG/PPG urethane) concentration are shown in Figure 2E. For
16 concentration higher than the CMC, the mean count rates reduced linearly with decreasing
17 poly(lignin/PEG/PPG urethane) concentration. This implies that the dilution decreased the
18 number of micelles in the solution. At concentration below CMC, the mean count rates showed
19 an approximately constant value regardless of the change in concentration, suggesting no
20 micelle formation in this range of concentration. The CMC value of the poly(lignin/PEG/PPG
21 urethane) was obtained as ~ 0.027 wt%, determined by the intersection of the best fit lines
22 drawn through the data point.

23

24

25 **3.4 Antioxidant properties of poly(lignin/PEG/PPG urethane)**

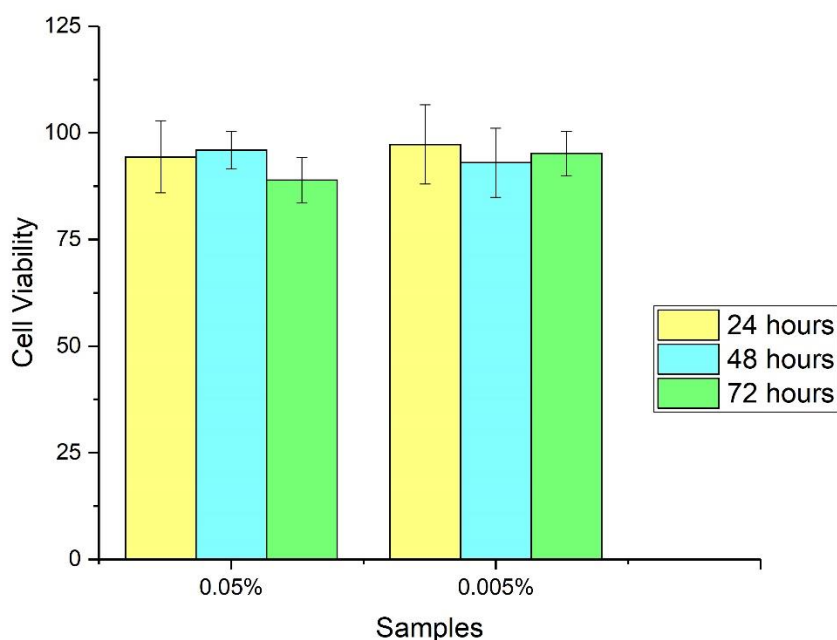
26 The antioxidant activities of poly(lignin/PEG/PPG urethane) were evaluated by DPPH assay.
27 As shown in Figure 2F, F127 had very low antioxidant activities with 27.9 ± 1.1 % free radical
28 inhibition even after 24 hours, while poly(lignin/PEG/PPG urethane) exhibited good
29 antioxidant properties. After one hour incubation, poly(lignin/PEG/PPG urethane) already
30 displayed very high free radical inhibition of $94.0 \pm 1.3\%$. Lignin is a natural antioxidant agent
31 and it contains a high content of phenolic moieties which can prevent the proliferation of free
32 radicals. Every day, our skin is exposed to damage from all kinds of free radical compounds.
33 The presence of these free radicals in the skin could cause skin damage, ranging from aging,
34 pigment darkening to skin cancer^[12]. The application of poly(lignin/PEG/PPG urethane) could

1 terminate the propagation of free radicals and potentially reduce localized oxidative stress in
2 our skin.

3
4

5 **3.5 Cytotoxicity Evaluation**

6 With the intention to use poly(lignin/PEG/PPG urethane) as a potential cosmetic, its
7 biocompatibility was investigated. Two concentrations were tested and it was incubated up to
8 72 hours with the cells. With reference to Figure 3, the results show that the developed
9 poly(lignin/PEG/PPG urethane) was highly compatible with the cells with more than 80% cell
10 viability detected even after 72 hours incubation.



11

12 Figure 3 Cell viability of 3T3 cells after 24h, 48h and 72h incubation with
13 poly(lignin/PEG/PPG urethane)

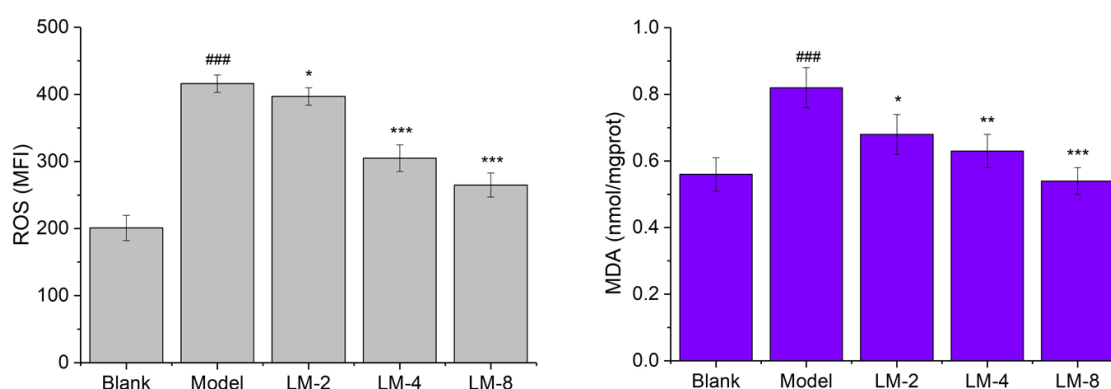
14 **3.6 ROS generation and MDA content in UVA-induced HSF cells**

15 While reactive oxygen species (ROS) are essential intermediates in oxidative metabolism,
16 excess ROS could induce undesirable oxidative stresses that damage cells by peroxidizing
17 lipids and disrupting structural proteins, enzymes and nucleic acids. With the aim to use
18 poly(lignin/PEG/PPG urethane) as the carrier for palmitoyl tripeptide-38 and also to provide
19 antioxidant activity, it would be relevant to examine if the encapsulation of the peptide would

1 affect the capability of the poly(lignin/PEG/PPG urethane) in serving its latter function. Hence,
 2 different concentrations of the peptides were encapsulated in the the poly(lignin/PEG/PPG
 3 urethane) micelles and the system would be subsequently referred to as LM. An indication of
 4 the antioxidant activity could be deduced from the amount of intercellular ROS generation,
 5 which was examined through the use of DCFH-DA fluorescence intensity measurement. As
 6 shown in Figure 4A, ROS generated by HSF cells exposed to UVA-alone (model group)
 7 attained 416 MFI, which was a 2.07-fold increment as compared to the control cells (not
 8 subjected to UVA irradiation and LM treatment). The treatment with 2, 4 and 8 $\mu\text{g}/\text{mL}$ of LM
 9 were shown capable of inhibiting UVA-induced ROS generation to 396.88 ± 12.55 ,
 10 305.05 ± 19.57 and 264.50 ± 17.91 , respectively.

11 Lipid peroxidation is a well-known process to indicate the oxidative stress in cells and tissues
 12 [13]. Free radicals degrade polyunsaturated fatty acids and generate malondialdehyde (MDA)
 13 [14]. Therefore, MDA is a widely used biomarker for lipid peroxidation and oxidative stress. As
 14 shown in Figure 4B, HSF cells exposed to UVA alone (model group) showed significant
 15 increase in MDA content from 0.56 ± 0.05 nmol/mgprot (control) to 0.82 ± 0.06 nmol/mgprot.
 16 The introduction of LM to the UVA-induced HSF cells showed a dose-dependent decrease in
 17 the MDA content and there was a statistically significant difference versus model group.

18 Hence, these results suggest that the poly(lignin/PEG/PPG urethane) is a suitable carrier for
 19 the palmitoyl tripeptide-38. The encapsulation of the peptides did not adversely affect its
 20 antioxidant properties.



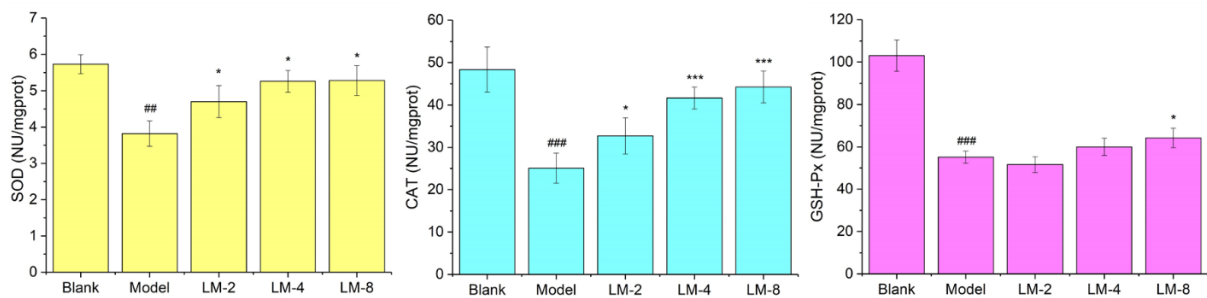
21
 22 Figure 4 Effect of LM on ROS generation (A) and MDA content (B) in UVA-induced HSF
 23 cells ###P<0.001 vs. the blank control; *P<0.05, ** P<0.01 and *** P<0.001 vs. the model group
 24 (UVA-alone)

1

2 3.7 Activities of SOD, CAT and GSH-Px in UVA-induced HSF cells

3 Three main antioxidant enzymes (Superoxide dismutase (SOD), catalase (CAT), and
4 glutathione peroxidase (GSH-Px)) in cells were selected to provide further insights into the
5 antioxidant activities of LM on HSF cells. These enzymes work together to defend against
6 oxygen-derived free radicals. SOD catalyses the conversion of superoxide anion into hydrogen
7 peroxide (H_2O_2), whereas CAT and GSH-Px reduce H_2O_2 into H_2O and O_2 [15]. Previous studies
8 have shown that SOD family could protect cells from UV radiation and the consequential skin
9 damage [16, 17]. CAT could reduce the damage to DNA caused by UV radiation [16, 18]. Hence,
10 antioxidant enzyme activities of SOD, CAT and GSH-Px were examined using relative kits to
11 evaluate the protective effect of LM on the antioxidant-defense system. Compared with the
12 control, SOD, CAT and GSH-Px activities of HSF cells exposed to UVA alone (model group)
13 significantly decreased to 3.82 ± 0.35 NU/mgprot, 25.08 ± 3.57 U/mgprot and 55.17 ± 2.80
14 U/mgprot respectively. The results were not surprising as it had been demonstrated that the
15 ultraviolet radiation could cause apoptosis and NETosis [19]. In contrary, UVA-induced HSF
16 cells treated with LM showed dose-dependent increase in SOD, CAT and GSH-Px activities
17 and statistically significant differences versus model group (Figure 5). In fact, LM-4 and LM-
18 8 appeared to have almost maintained the same level of SOD activity and CAT activity in the
19 cells as the control, that was not exposed to UVA irradiation. Thus, LM treatment was
20 considered to be effective in protecting the cells and its antioxidant defense system against UV
21 irradiation.

22



23 Figure 5 Effect of LM on SOD activity (A), CAT activity (B) and GSH-Px activity (C) in UVA-
24 induced HSF cells ###P<0.001 and ##P<0.01 vs. the blank control; *P<0.05 and ***P<0.001 vs.
25 the model group (UVA-alone)

26

27

1 3.8 Effect of LM on UVA-induced cytotoxicity in HSF cells

2 In order to further substantiate the UV shielding of LM and the explanation for the drop in the
3 level of antioxidant enzyme activities, CCK-8 assay and LDH activity measurements were
4 performed. As shown in Table 1, UVA exposure significantly reduced HSF cell viability to
5 50.59% as compared with the control cells. In contrast, the viability of HSF cells increased
6 along with the applied LM concentration achieving 55.87%, 65.40% and 71.98% with the use
7 of LM containing 2, 4 and 8 $\mu\text{g/mL}$ of palmitoyl tripeptide-38 respectively. Correspondingly,
8 LDH activity in UVA-induced HSF cells decreased significantly with increasing concentration
9 of LM (Table 1). LDH is an important marker associated with tissue damage in our body as it
10 is only released substantially during injuries and diseases. Our results demonstrate that LM had
11 the capability to protect HSF cells from UV irradiation.

12 Table 1. Effect of LM on UVA-induced cytotoxicity in HSF cells

Samples	Absorbance value(OD 450nm)	Survival rate	LDH (U/L)
Blank	1.84 ± 0.02	100%	533 ± 57
Model group	$0.93 \pm 0.03^{###}$	50.59%	$1629 \pm 97^{###}$
LM-2	$1.03 \pm 0.05^*$	55.87%	$1323 \pm 139^{**}$
LM-4	$1.20 \pm 0.01^{***}$	65.40%	$827 \pm 67^{***}$
LM-8	$1.32 \pm 0.03^{***}$	71.98%	$703 \pm 43^{***}$

13 $^{###} P < 0.001$ vs. the blank control; $^* P < 0.05$ and $^{***} P < 0.001$ vs. the model group (UVA-alone).

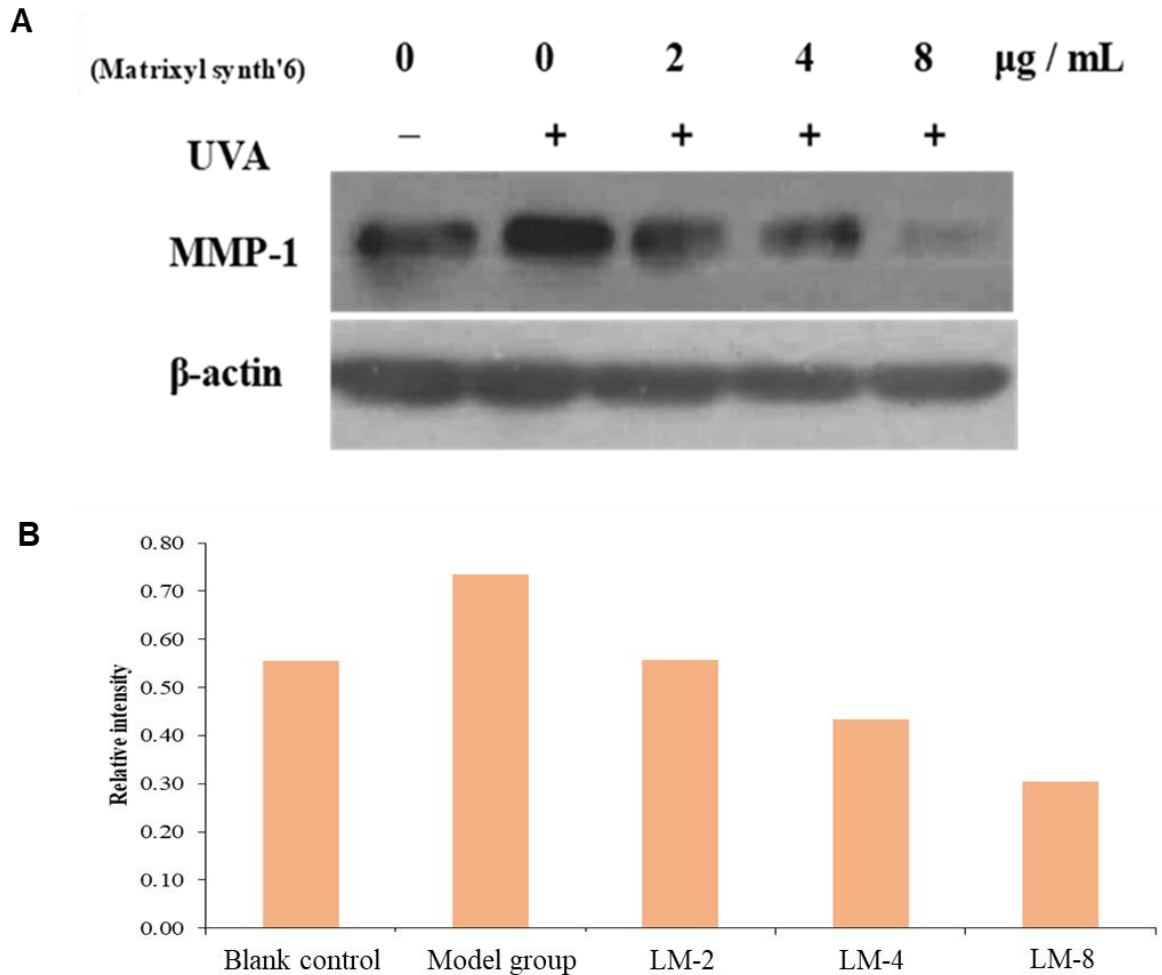
14

15 3.9 Expression of MMP-1 in UVA-induced HSF cells

16 Besides inducing the ROS generation, the exposure to sunlight also elevates the matrix
17 metalloproteinase-1 (MMP-1) content ^[20], which is the enzyme responsible for collagen
18 digestion. Collagen is one of the main structural substance in our body and also, our skin.
19 Collagen fibers established the matrix of our skin providing integrity, firmness and elasticity
20 to the structure. Therefore, a high level of MMP-1 is usually associated with photoaging. In
21 order to achieve maximum anti-aging effect, it would be advantageous for the treatment to

1 target both ROS generation as well as the expression of MMP-1. In our investigation, it appears
 2 that the increased encapsulation of palmitoyl tripeptide-38 led to decline in MMP-1 expression
 3 (Figure 6A and Figure 6B). These results suggest good efficacy of LM in reducing MMP-1
 4 expression, which could possibly translate to lesser collagen digestion.

5



6

7 Figure 6 Expression of MMP-1 in UVA-induced HSF cells (A) and its relative intensity of
 8 expression after treated with different dosages of palmitoyl tripeptide-38 (B)

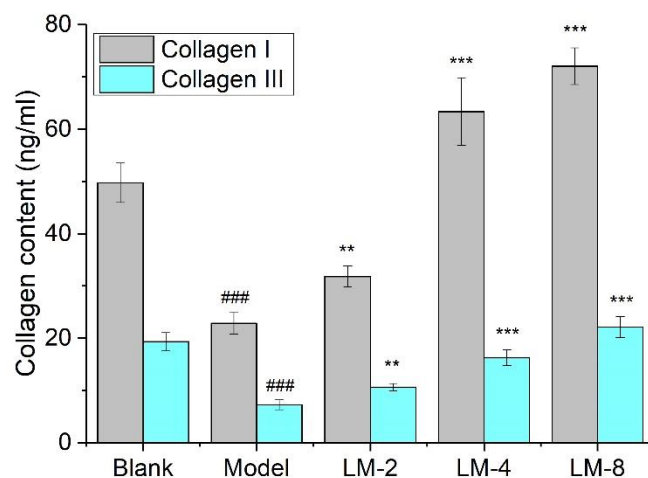
9

10 **3.10 Collagen content in UVA-induced HSF cells**

11 Next, study was performed to assess if the effect of palmitoyl tripeptide-38 was successfully
 12 delivered via LM. There are many types of collagen in our body, each serving a different
 13 function to support the normal functioning of the body. The collagen present in the skin are
 14 predominantly collagen type I and III. In this study, ELISA assay was conducted to examine

1 the ability of LM to maintain the collagen contents in the HSF cells after subjected to UVA
 2 irradiation. As shown in Figure 7, UVA exposure of HSF cells significantly reduced type I
 3 collagen content to 22.86 ± 2.07 ng/mL as compared with the control cells. The groups that
 4 were treated with 2, 4 and 8 $\mu\text{g/mL}$ of LM were observed with higher type I collagen content
 5 in UVA-induced HSF cells, which was attained up to 31.81 ± 2.05 , 63.37 ± 6.48 and $72.06 \pm$
 6 3.5 ng/mL respectively. Similarly, UVA exposure significantly reduced type III collagen
 7 content in HSF cells from 19.32 ± 1.7 ng/mL to 7.28 ± 0.94 ng/mL (Figure 7). In contrast, the
 8 type III collagen content in UVA-induced HSF cells treated with LM at concentrations of 2, 4
 9 and 8 $\mu\text{g/mL}$ increased significantly to 10.65 ± 0.67 , 16.24 ± 1.49 and 22.15 ± 2.01 ng/mL
 10 respectively.

11 It was noteworthy that the collagen I content obtained after LM-4 and LM-8 treatment
 12 exceeded the control group. The intended function of palmitoyl tripeptide-38 displayed through
 13 the elevated collagen I content signifies that poly(lignin/PEG/PPG urethane) is a suitable
 14 peptide carrier. Additionally, palmitoyl tripeptide-38 has been demonstrated previously as a
 15 powerful peptide to promote the production of collagen type I in *in vitro* cell culture studies.
 16 Hamley et al. reported that 80 $\mu\text{g/mL}$ of palmitoyl tripeptide-38 doubled the collagen content
 17 produced from human corneal and dermal fibroblasts as compared with the basal media [3].
 18 Compared to their findings, our LM with 10-time lower concentration (8 $\mu\text{g/mL}$) was able to
 19 increase 3 times of collagen production even after UV treatment. This result indicated that the
 20 LM capsules could not only protect skin cells from UV damage, but also stimulate the cells to
 21 release more collagen for skin repair.



1 Figure 7 Effect of LM on type I and type III collagen content in UVA-induced HSF cells
2 ###P<0.001 vs. the blank control; **P<0.01 and *** P<0.001 vs. the model group (UVA-alone)

3

4 **4 Conclusion**

5 In this work, a lignin-based carrier was developed to deliver palmitoyl tripeptide-38 into the
6 cells overcoming the penetrating difficulty of large peptide. The two-way approach utilized in
7 this study placed the emphasis on simultaneously minimizing damages and promoting repair.
8 It seems promising with the decreased ROS generation, MDA content and MMP-1 expression.
9 UVA-induced HSF cells treated with LM showed dose-dependent increase in SOD, CAT and
10 GSH-Px activities. Higher cell viability and reduced LDH activity were associated with higher
11 concentration of LM used. Additionally, the established system promoted the collagen
12 production for skin repair. It was noteworthy that the collagen I content obtained after LM-4
13 and LM-8 treatment exceeded that of the control. Hence, this work successfully demonstrated
14 a possible way to valorize lignin to sustainable peptide carrier, that exhibited good antioxidant
15 properties without adverse effect on the peptide.

16

17 **CRedit authorship contribution statement**

18 Pei Lin Chee: Investigation, Methodology, Visualization, Writing – original draft, Formal
19 analysis. Sigit Sugiarto, Yu Yong & Tan Ying Chuan: Investigation, Methodology, Writing –
20 original draft. Enyi Ye: Investigation, Methodology, Conceptualization. Dan Kai: Supervision,
21 Methodology, Writing – review & editing, Conceptualization, Validation. Xian Jun Loh:
22 Conceptualization

23

24 **Conflicts of interest**

25 There are no conflicts to declare.

26

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2 Technology and Research (A*STAR).
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